

1 **In Vitro Safety and Quality of Magnetically Labeled Human Mesenchymal**
2 **Stem Cells Preparation for Cartilage Repair**

3
4 Short title: Assessments of MSC for magnetic targeting

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6 Hiroshi Negi, MD,¹ Syunsuke Takeuchi,² Naosuke Kamei, MD, PhD,^{1,3} Shinobu
7 Yanada, PhD,² Nobuo Adachi, MD, PhD,¹ Mitsuo Ochi, MD, PhD⁴

8
9 Affiliations and institutional mailing addresses

10 ¹ Department of Orthopaedic Surgery, Graduate School of Biomedical & Health Sciences,
11 Hiroshima University, Hiroshima University, Hiroshima, Japan.

12 ² Japan Tissue Engineering Co., Ltd., Gamagori, Japan.

13 ³ Medical Center for Translational & Clinical Research, Hiroshima University Hospital,
14 Hiroshima, Japan.

15 ⁴ President of Hiroshima University, Higashihiroshima, Japan.

16
17 Contract information:

18 Hiroshi Negi: 1-2-3 Kasumi, Minami-ku, Hiroshima 734-8551, Japan, Phone: (+81) 82-
19 257-5233, FAX: (+81) 82-257-5234, E-mail: kamonegi1983@yahoo.co.jp

20 Syunsuke Takeuchi: 6-209-1 Miyakitadori, Gamagori, Aichi 443-0022, Japan, Phone:
21 (+81) 533-66-2020, FAX: (+81) 533-66-2019, E-mail: syunsuke_takeuchi@jpte.co.jp

22 Naosuke Kamei: 1-2-3 Kasumi, Minami-ku, Hiroshima 734-8551, Japan, Phone: (+81)
23 82-257-5233, FAX: (+81) 82-257-5234, E-mail: nahkamei@hiroshima-u.ac.jp

24 Shinobu Yanada: 6-209-1 Miyakitadori, Gamagori, Aichi 443-0022, Japan, Phone: (+81)

25 533-66-2020, FAX: (+81) 533-66-2019, E-mail: shinobu_yanada@jpte.co.jp

26 Nobuo Adachi: 1-2-3 Kasumi, Minami-ku, Hiroshima 734-8551, Japan, Phone: (+81) 82-

27 257-5233, FAX: (+81) 82-257-5234, E-mail: nadachi@hiroshima-u.ac.jp

28 Mitsuo Ochi: 1-3-2 Kagamiyama, Higashihiroshima 739-8511, Japan, Phone: (+81) 82-

29 424-6006, FAX: (+81) 82-424-6007, E-mail: ochim@hiroshima-u.ac.jp

30

31 Corresponding author: Naosuke Kamei, MD, PhD

32

33 **Abstract**

34 Magnetic delivery of mesenchymal stem cells (MSCs) has been developed for cartilage
35 repair. It provides an effective and minimally invasive method for MSC transplantation.
36 In this study, we evaluated the safety and quality of magnetically labeled human MSCs
37 for practical applications. The safety of magnetically labeled MSCs was assessed using
38 karyotyping, colony-forming assay using soft agar, and cell proliferation in a long-term
39 culture. Magnetic labeling did not affect the karyotype, and MSCs retained the ability to
40 grow and proliferate in an anchorage-independent manner even after exposure to
41 magnetic force. The quality of the magnetically labeled MSCs was assessed by
42 chondrocyte differentiation and reactivity towards magnetic forces. Magnetic labeling
43 inhibited the chondrogenic differentiation of MSCs at higher densities of magnetic
44 particles. MSCs labeled with ferucarbotran nanoparticles were retained by magnetic
45 forces in a dose- dependent manner. The magnetization of MSCs with a proper density of
46 magnetic particles maintained both qualities in MSCs. However, the uptake quantity of
47 iron into MSCs varied across donors, even for the same density of magnetic particles.
48 Therefore, the proper density of magnetic particles for use in MSC delivery for cartilage
49 repair should be examined for every donor before treatment.

50

51 **Impact Statement**

52 This study is very important as a preclinical assessment of the safety and quality
53 assessments of magnetically labeled MSCs for use in cartilage repair. The findings of this
54 study show that magnetic labeling with an appropriate density of magnetic particles has
55 no harmful effects on the safety and quality of MSCs.

56

57 **Introduction**

58 Mesenchymal stem cells (MSCs) have been widely used in regenerative medicine from
59 animal models to clinical trials. A particularly useful application of MSCs has been
60 cartilage repair, as MSCs possess a chondrocyte differentiation capacity (1, 2). A
61 magnetic delivery system for MSCs, termed magnetic targeting, has been previously
62 developed for the treatment of articular cartilage defects (3). In this cell delivery system,
63 superparamagnetic iron oxide (SPIO) nanoparticles (ferucarbotran) are incorporated into
64 the cytoplasm of MSCs for magnetic cell labeling. Magnetically labeled MSCs are then
65 injected into a joint, where they can be controlled and accumulated in a cartilage lesion
66 by the use of magnetic forces. The efficacy and safety of this treatment for articular
67 cartilage repair have been reported in a miniature swine model as well as a clinical trial
68 (4, 5). The safety and quality assessments of bone marrow MSCs for articular cartilage
69 repair have also been reported (6, 7). However, for magnetically labelled human MSCs
70 such an assessment has never been reported. Therefore, a safety and quality evaluation of
71 magnetically labeled human MSCs is highly warranted before realizing the practical
72 application of magnetic targeting. The purpose of this study is to clarify the effect of
73 magnetic labeling on the safety and quality of human bone marrow MSCs, for use in
74 cartilage regeneration therapies.

75

76 **Materials and methods**

77 *Human bone marrow MSCs*

78 In this study, commercially available human bone marrow MSCs were purchased (PT-
79 2501; Lonza, Walkersville, MD). MSCs from eight donors were used in this study (Lot
80 number: 1F4287 from a 22-year-old male, 2F3478 from a 43-year-old male, 296578 from

81 a 45-year-old male, 310956 from a 24-year-old female, 318006 from a 27-year-old male,
82 326162 from a 38-year-old male, 429365 from a 30-year-old male, and 451491 from a
83 25-year-old male). All these MSCs passed the quality inspection conducted by Lonza
84 company using cell viability (more than 75%), adipogenic and osteogenic differentiation
85 ability (Oil Red O Staining and Calcium Deposition Staining), and flow cytometric
86 analysis of cell surface markers (more than 90 % were positive for CD29, CD44, CD105,
87 and CD166, and less than 10 % were positive for CD14, CD34, and CD45). Six of these
88 lots (Lot numbers: 1F4287, 2F3478, 296578, 310956, 318006, 326162) were used for
89 safety assessments including karyotype analysis, proliferation capacity in long-term
90 culture, colony forming assay in soft agar and quantification of magnetic labeling. On the
91 contrary, three of these lots (1F4287, 429365, and 451491) were used for quality
92 assessments including viability, content of iron, the reactivity for magnetic attractive force,
93 and chondrogenic differentiation capacity of MSCs.

94 *Culture of MSCs*

95 Human bone marrow MSCs at passage 2 (P2) were centrifuged at 1200 rpm for 5 minutes
96 and resuspended in culture medium, containing Dulbecco's modified Eagle medium
97 (DMEM, Thermo Fisher Scientific, Waltham, MA), 15 % fetal bovine serum (FBS,
98 Sigma-Aldrich, St. Louis, MO), 20 mmol/mL 4-(2-hydroxyethyl)-1-
99 piperazineethanesulfonic acid (HEPES, Thermo Fisher Scientific), 50 µg/mL gentamycin
100 (Gentacin®, MSD, Kenilworth, NJ), and 0.25 µg/mL amphotericin (Fungizon®, Bristol-
101 Myers Squibb, New York, NY). The MSCs were seeded at a density of 3,500–5,000
102 cells/cm² onto 10 cm culture dishes and cultured at 37 °C with 5% CO₂. The culture
103 medium was changed every 4 days. On reaching sub-confluence, the cells were harvested
104 with trypsin (TrypLE™ select, Thermo Fisher Scientific), and reseeded. The proliferation

105 capacity of MSCs was examined by long-term culture. The MSCs were cultured until
106 their number decreased for two successive passages during long-term culture.

107 *Magnetic Labeling of MSCs*

108 On reaching 70% confluence, the MSCs were magnetically labeled with ferucarbotran
109 (Rizovist[®], FUJIFILM RI Pharma, Tokyo, Japan). The MSCs were incubated in culture
110 medium containing ferucarbotran at a concentration of 97.6 µg iron (Fe)/mL for 12
111 hours in a standard method (Fe x1, 12 hours). As a severe condition, MSCs were
112 magnetically labeled in 2 types of different conditions including 195 µg Fe/mL labeling
113 medium for 12 hours (Fe×2, 12 hours) and 97.6 µg Fe/mL labeling medium for 36 hours
114 (Fe×1, 36 hours) for long-term culture. For the quality assessment of MSCs,
115 ferucarbotran was added to the MSC culture at P3. The MSCs were incubated in the
116 culture medium containing ferucarbotran at six different concentrations for 12 hours.
117 The concentration of 97.6 µg Fe/mL was defined as the standard dose (standard group),
118 whereas the other concentrations were defined as follows; control group (0 µg Fe/mL),
119 one-quarter group (24.4 µg Fe/mL), one-half group (48.8 µg Fe/mL), three-quarters
120 group (73.2 µg Fe/mL), and double-dose group (195 µg Fe/mL). After the incubation for
121 magnetic labeling, all the cells were washed thrice with sterile phosphate buffered saline
122 (PBS) and used for assays.

123 *Exposure of MSCs to magnetic field*

124 A portion of the standard-dose MSCs were exposed to a magnetic field for the safety
125 assessments. A superconducting magnetic device was used for this purpose (4) (Fig.
126 1A). Magnetically labeled MSCs were suspended in 3 mL of culture medium in a 50-
127 mL polypropylene tube. The tube was placed at the center of the magnetic field

128 generated from the device for 10 minutes. The exposure to the labeled MSCs as 0.55–
129 5.48 tesla (T), considering the size of the tube and magnetic flux distribution (Fig. 1B).
130 The labeled MSCs were aggregated in the tube because of the magnetic force (Fig. 1C).
131 They were re-suspended by gentle pipetting, and used for safety assessments including
132 karyotype analysis, soft agar assay, and long-term culture.

133 *Karyotype Analysis*

134 The karyotypes of the labeled MSCs was analyzed by the G-banding technique. For
135 each sample, 20 or 50 metaphase cells were analyzed. The chromosomes were analyzed
136 by visual inspection. In the assessment before the exposure to the magnetic field, the
137 MSCs were labeled at P2 and at P5 and analyzed at P5 (n = 20 cells). In the assessment
138 after the exposure to the magnetic field, the MSCs were labeled at P5 and analyzed at
139 P5 and P10 (n = 50 cells).

140 *Culture in soft agar*

141 Before and after the exposure to the magnetic field, 1×10^4 MSCs (labeled at P5 and
142 analyzed at P5) were mixed with the culture medium containing 0.33% agar and
143 overlaid on 0.5% agar in a 60-mm culture dish. The cells were cultured for 21 days.
144 HeLa-S3 cells and MRC-5 cells were used as positive and negative control,
145 respectively. The viability of the cells was confirmed by observing their ability to form
146 a colony within 14 days. The assay was performed in triplicate.

147 *Quantification of magnetic labeling*

148 Quantification of the magnetic labeling of MSCs was performed on cytopsin slides. The
149 cell suspension was transferred to disposable cytofunnels with attached cytopsin slides
150 and spun at 1000 rpm for 5 minutes in a Cytospin4 Cyto centrifuge (Thermo Fisher

151 Scientific). The slides were then fixed in 4 % paraformaldehyde for 20 minutes and
152 washed with phosphate buffer. The cells on the slides were stained with Berlin blue
153 (FUJIFILM Wako Pure Chemical Corporation, Osaka, Japan) and counterstained with
154 Kernechtrot (Muto Pure Chemicals, Tokyo, Japan). The labeling index was calculated
155 by dividing the total blue intensity in the cell area in 10 pictures by the cumulative cell
156 number. The blue intensity in pictures was estimated by computerized measurement
157 (WinROOF, version 7.0, Mitani Co., Tokyo, Japan). The labeling index of each passage
158 was normalized with the values obtained immediately after magnetic labeling and
159 displayed as a relative value.

160 *Cell viability*

161 Following the magnetic labeling, MSCs at P4 were collected after trypsinization and
162 suspended in 1 mL of PBS. A 10- μ L volume of this solution was mixed with 0.4 %
163 (w/v) Trypan Blue Solution (FUJIFILM Wako Pure Chemical Corporation) and the
164 viability of MSCs labeled with different magnetic concentrations was evaluated using
165 cell counter (TC10TM Automated Cell Counter; BIO-Rad Laboratories, CA).

166 *Iron Content in MSCs*

167 Lysates were made from magnetically labeled MSCs from three different donors at six
168 different concentrations of ferucarbotran for 12 hours. The iron content of the lysate was
169 measured using Metallo Assay kit (Metallo Assay; Metallogenics, Chiba, Japan). The
170 MSCs in each experimental group were first counted, following which, they were
171 homogenized in cell lysate buffer using ultrasonic sonicator. The crude lysate thus
172 obtained was then mixed with HCl (0.01 M final concentration) and incubated at 20 °C
173 for 30 min. The lysate was then centrifuged at 4 °C for 15 minutes, and the supernatant

174 was quantified according to the manufacturer's instructions. The iron content was
175 expressed as pg/cell.

176 *Assessment of chondrogenic differentiation capacity*

177 Chondrogenic differentiation ability of the MSCs from each donor was evaluated using
178 pellet culture, according to Sekiya's method (8-10). About 2.5×10^5 of MSCs at P4 was
179 centrifuged at 450 g for 10 minutes using 15-mL polyethylene terephthalate tube. The
180 pellet was cultured at 37 °C with 5 % CO₂ in 500 µL of chondrogenic medium containing
181 500 ng/mL bone morphogenetic protein (BMP)-6 (R&D Systems, Minneapolis, MN) in
182 addition to high-glucose DMEM supplemented with 10 ng/mL TGF-β₃ (R&D Systems),
183 10^{-7} M dexamethasone, 50 µg/mL ascorbate-2-phosphate, 40 µg/mL proline, 100 µg/mL
184 pyruvate (Sigma-Aldrich), and 50 mg/mL ITS+ Premix (6.25 µg/mL insulin, 6.25 µg/mL
185 transferrin, 6.25 ng/mL selenous acid, 1.25 mg/mL bovine serum albumin, and 5.35
186 mg/mL linoleic acid; Becton Dickinson, Franklin Lakes, NJ). The medium was replaced
187 every 3 to 4 days for 21 days. For each concentration of the m-MSCs (magnetic MSCs),
188 the long diameter of the spheroids was measured. For histological evaluation under
189 microscopy, the pellets were embedded in paraffin, cut into 5-µm sections, and stained
190 with 0.05 % toluidine blue solution and Safranin-O/Fast green.

191 For the glycosaminoglycan (GAG) quantification, the pellets were digested in 3000
192 units/mL Collagenase (Merck, Darmstadt, Germany) and 0.25 % Trypsin (Thermo Fisher
193 Scientific). After 30 minutes of digestion, the homogenate was centrifuged at 12,000 rpm.
194 for 10 minutes. The GAG content of the supernatant was measured using Blyscan
195 Glycosaminoglycan Assay Kit (Funakoshi, Tokyo, Japan) according to the
196 manufacturer's instructions.

197 In addition, mRNA expression levels of collagen type II (COL II, *COL2A1*) were
198 evaluated. Total RNA was isolated from pellets using a Qiagen RNeasy Micro Kit
199 (Qiagen, Valencia, CA). cDNA was synthesized from the RNA using Super Script VILO
200 Master Mix (Thermo Fisher Scientific). As a control, total RNA was isolated from
201 normal knee cartilage dissected from skeletally matured cadaveric donors (Articular
202 Engineering, Northbrook, IL). qPCR was performed using Power SYBR Green Master
203 Mix (Thermo Fisher Scientific). cDNA samples were analyzed for both *COL2A1* and
204 the reference gene (glyceraldehyde-3-phosphate dehydrogenase (*GAPDH*)). The assays
205 were performed according to the manufacturer's instructions. The mRNA expression of
206 *COL2A1* was normalized to that of *GAPDH*.

207 *Reaction of MSCs to magnetic attractive force*

208 Reactivity of MSCs towards magnetic attractive force under the six treatments (0, 24.4,
209 48.8, 73.2, 97.6, and 195 $\mu\text{g Fe/mL}$) was measured using a method described in the
210 MACS manual separator (Miltenyi Biotec, Cologne, Germany) (11). Micro fluidics chip
211 (Sumitomo Bakelite Co, Tokyo, Japan) and four different magnetic flux densities of the
212 neodymium magnet (20 mT, 100 mT, 250 mT, and 500 mT) were used. The neodymium
213 magnet was placed at the center of the column. The cell density was maintained at
214 3.0×10^5 cells/mL and 2 μL of cell solution was injected into one hole. The flow of the
215 cell solution was measured under the influence of magnetic force, as well as without the
216 magnetic force (Fig. 2).

217 *Statistical Analysis*

218 All the results were compared between the examination groups and the donor groups.
219 Statistical analysis was performed using software Statcel4; a statistical program for

220 performing statistics in MS Excel (Statcel4: Nebula Company, Tokyo, Japan). The
221 results are represented as mean value \pm standard deviation (SD). Multiple comparisons
222 were performed for all experiments using a single factor ANOVA and Bartlett's test.
223 When the p-value was significant, the Turley-Kramer method was used to find the
224 pairwise differences among groups.

225

226 **Results**

227 *Karyotype of MSCs*

228 Three lots of human MSCs were used for karyotype analysis (1F4287, 2F3478,
229 296578). The karyotype was analyzed in P2 and P5 MSCs without labeling, P5 MSCs
230 labeled at P2, and P5 MSCs labeled at P5. No abnormalities were seen in 2F3478 and
231 296578 in any of the conditions. Although P2 and P5 MSCs without labeling and P5
232 MSCs labeled at P2 were also normal in 1F4287, 2 of the 20 P5 MSCs labeled at P5 in
233 1F4287 had an abnormality, balanced reciprocal translocation between chromosome 13
234 and chromosome 10 (Fig3 A-C). To verify whether this abnormality in 1F4287 was
235 caused by labeling, the karyotype of MSCs in 1F4287 was reanalyzed. P5 MSCs labeled
236 at P5 (n = 50) and P10 MSCs labeled at P5 (n = 50) were analyzed and no abnormalities
237 were observed. (Fig. 3 D, E).

238 *Proliferation of magnetically labeled MSCs*

239 Three lots of human MSCs were used for proliferation assessments (1F4287, 2F3478,
240 296578). Proliferation capacity was examined using long-term culture of MSCs of the
241 four labeling treatments (control MSCs without labeling, Fe \times 1, 12 hours; MSCs labeled
242 with 97.6 μ g Fe/mL labeling medium for 12 hours, Fe \times 2, 12 hours; MSCs labeled with

243 195 µg Fe/mL labeling medium for 12 hours, Fe×2, 12 hours; and MSCs labeled with
244 97.6 µg Fe/mL labeling medium for 36 hours). Initially, magnetic labeling promoted a
245 slight proliferation of MSCs in all lots. Especially, MSCs of donor 0000296578 have 5-
246 10 more population doublings after prolonged or 2x concentration incubation with
247 ferucarbotran. However, MSCs of all treatments finally lost their proliferation capacity in
248 all lots (Fig. 4).

249 To evaluate the anchorage-independent growth of MSCs, P5 MSCs labeled at P5
250 were cultured in soft agar. While the positive control cells (HeLa-S3) formed colonies in
251 soft agar, the negative control cells (MRC-5) and MSCs from any of the donors did not
252 form colonies (data not shown).

253 *Effect of exposure to magnetic field on the safety of MSCs*

254 All the safety examinations were performed after a 10-min exposure of MSCs to magnetic
255 field for using the same three lots of MSCs as above (1F4287, 2F3478, and 296578) as
256 well as an additional 3 lots (310956, 318006, and 326162). The karyotype of 50 P5 MSCs
257 labeled at P5 (1F4287, 2F3478, and 296578) were examined. No abnormalities were
258 observed in the magnetically labeled MSCs (Fig. 5A). In addition, the P5 MSCs labeled
259 at P5 (1F4287, 2F3478, 296578) did not form any colony when cultured in soft agar (data
260 not shown).

261 Further, the proliferation capacity of MSCs (310956, 318006, and 326162) exposed to
262 magnetic field in a long-term culture under four type of conditions (-Fe, -Mg: MSCs
263 without magnetic-labeling and exposure to magnetic field; -Fe, +Mg: MSCs without
264 magnetic-labeling exposed to magnetic field; +Fe, -Mg: magnetic-labeled MSCs without
265 exposure to magnetic field; and +Fe, +Mg: magnetic labeled MSCs exposed to magnetic
266 field). MSCs of donor 0000326162 have 3 more population doublings upon incubation

267 with ferucarbotran than without ferucarbotran. However, the proliferation of all these
268 MSCs ceased within 100 days (Fig.5B).

269 These findings indicated that exposure to magnetic field does not cause malignant
270 transformation in magnetically labeled MSCs.

271 *Release of iron particles from MSCs*

272 Three lots of MSCs (1F4287, 2F3478, and 296578) were magnetically labeled under three
273 types of conditions. After the magnetic labeling, the percentage of magnetically labeled
274 MSCs was measured during culture using Berlin blue staining for all three types of
275 labeling conditions (Fe x1, 12 hours; MSCs labeled with 97.6 $\mu\text{g Fe/mL}$ labeling
276 medium for 12 hours, Fe \times 2, 12 hours; MSCs labeled with 195 $\mu\text{g Fe/mL}$ labeling
277 medium for 12 hours, Fe \times 2, 12 hours; and MSCs labeled with 97.6 $\mu\text{g Fe/mL}$ labeling
278 medium for 36 hours). Hundred percent of MSCs were magnetically labeled at the start
279 of culture. However, the percentage of the magnetically labeled MSCs decreased with
280 time (Fig. 6A), and they became rare after culturing for more than 2 or 3 weeks in all
281 lots under all conditions. (Fig. 6B)

282 *Viability of MSCs*

283 Three lots of MSCs (1F4287, 429365, and 451491) were used for the quality
284 assessments including viability, iron content, the reactivity towards magnetic attractive
285 force, and chondrogenic differentiation capacity of MSCs. For the quality assessments,
286 the magnetic labeling conditions were defined as follows: control group (0 $\mu\text{g Fe/mL}$),
287 one-quarter group (24.4 $\mu\text{g Fe/mL}$), one-half group (48.8 $\mu\text{g Fe/mL}$), three-quarters
288 group (73.2 $\mu\text{g Fe/mL}$), standard group (97.6 $\mu\text{g Fe/mL}$), and double-dose group (195
289 $\mu\text{g Fe/mL}$).

290 The average viability of MSCs was $90.1\pm 6.6\%$. There were no significant differences
291 in cell viability among the donors under any of the conditions (data not shown).

292 *Iron Content in MSCs*

293 The iron content increased gradually, with increasing concentration of ferucarbotran in
294 the MSCs from all donors. (Fig. 7) On an average, in three donors, the iron content
295 increased proportionally to the concentration of ferucarbotran in the medium to half the
296 standard concentration, and saturated at three quarters of the standard concentration or
297 higher. However, there were differences in iron contents among the magnetically
298 labeled MSCs from different donors. These findings suggest that the capacity for
299 ferucarbotran uptake into MSCs varies with the donor.

300 *Chondrogenic differentiation of MSCs*

301 The chondrogenic differentiation capacity of MSCs was assessed using pellet culture.
302 The long diameter of spheroids from donor 429365 was especially smaller than the others.
303 (Fig. 8) Histologically, metachromasia was observed at every concentration of iron, but
304 the toluidine blue and safranin-O stainabilities of the pellets from all donors in the double-
305 dose group were lower than those of the other groups (Fig. 8). For the quantitative
306 assessments of chondrogenic differentiation, the expressions of GAG and COL II mRNA
307 were measured. The GAG expression in the MSCs from donor 429365 was decreased in
308 the three-quarters group and the standard group (n=1). However, GAG quantification
309 increased in the double-dose group (Fig. 9A). Too high concentration of iron in the
310 double-dose group might have induced an error in the absorbance measurement of GAG.
311 The mRNA expression level of COL II from donor 429365 decreased in the three-quarters
312 group and the higher concentration groups (Fig. 9B). On the contrary, the expressions of

313 GAG and COL II mRNA from donors 1F4287 and 451491 decreased only in the double-
314 dose group (Fig.9 A, B). These findings showed that the chondrogenic differentiation
315 capacity of MSCs was maintained at the standard concentration of iron for donors 1F4287
316 and 451491, and at one-half concentration of iron for donor 429365.

317 *Reactivity of the MSCs towards magnetic force*

318 In the control group (0 mT), there were no differences in the cell number across
319 concentrations, but as the flux density of the magnet increased, the number of cells not
320 attracted to the magnet decreased. The cell numbers decreased depending on the density
321 of magnetic flux and the iron concentration. A magnetic flux density of 100 mT or
322 higher was required to decrease the cell number in all donors. At a magnetic density of
323 100 mT, one-half concentration of iron was enough to decrease the cell number in donor
324 429365. However, the standard concentration of iron was required to decrease the cell
325 number in donors 1F4287 and 451491 (Fig. 10).

326

327 **Discussion**

328 This study demonstrated that magnetic labeling did not impair the safety of MSCs as
329 assessed by karyotyping, colony-forming assay in soft agar, and cell proliferation in long-
330 term culture. Although magnetic labeling inhibited the chondrogenic capacity of MSCs,
331 an appropriate concentration of iron was able to maintain their chondrogenic
332 differentiation capacity as well as their reactivity towards magnetic force. The appropriate
333 concentration of iron for the magnetic labeling of MSCs varied according to the donor.

334 For one of the three donors (1F4287), the karyotype analysis showed an abnormality
335 in 2 out of the 20 P5 MSCs labeled at P5. However, the second karyotype analysis of

336 MSCs for 1F4287 (P5 MSCs labeled at P5 and P10 MSCs labeled at P5) failed to show a
337 single abnormality among 50 cells. It is known that chromosomal instability of MSCs
338 occurs in normal culture (12). Therefore, the abnormality observed in lot 1F4287 was
339 considered a rare, occasional event that occurred independent of the labeling. Magnetic
340 labeling promoted the proliferation of MSCs in the long-term culture. A previous study
341 also showed that the proliferation activity of the magnetically labeled MSCs was slightly
342 higher than that of the non-labeled MSCs (13), however, the magnetically labeled MSCs
343 finally lost their proliferation capacity similar to the non-labeled MSCs as observed in the
344 present study. In addition, the magnetically labeled MSCs never formed colonies in soft
345 agar. These findings suggest that magnetic labeling does not cause malignant
346 transformation of MSCs. Even a 10-min exposure of magnetically labeled MSCs from
347 the same three donors to a magnetic field did not show any abnormality in karyotyping,
348 colony-forming assay using soft agar, or cell proliferation in a long-term culture.
349 Therefore, we concluded that the magnetic labeling and exposure to magnetic field did
350 not adversely affect the safety of MSCs.

351 In the assessment of the percentage of magnetically labeled MSCs during culture using
352 Berlin blue staining, almost all MSCs were labeled just after labeling. However, the
353 percentage of magnetically labeled MSCs markedly decreased within 2 or 3 weeks. This
354 property might be advantageous for ensuring safety after transplantation, because iron
355 particles will not permanently remain at the transplanted site. However, the *in vivo*
356 kinetics of ferucarbotran after transplantation should be clarified.

357 During the quality assessment, magnetic labeling did not affect the viability of MSCs
358 regardless of the ferucarbotran concentration. However, magnetic labeling using high-
359 density ferucarbotran inhibited the chondrogenic differentiation of MSCs. A previous

360 study reported that magnetic labeling at a concentration of 100 $\mu\text{g Fe/mL}$ does not affect
361 the chondrogenic differentiation of MSCs (14). Kamei et al. showed, using a mini-pig
362 model, that the magnetic delivery system with a standard dose of ferucarbotran was better
363 than the control for the regeneration of hyaline cartilage in cartilage defects (4). On the
364 contrary, Henning and Bulte showed that chondrogenic differentiation of m-MSCs in
365 cartilage defects was inhibited by iron in a concentration-dependent manner (15, 16). Iron
366 oxide nanoparticles have been widely reported to produce highly reactive hydroxyl
367 radicals (17) . These radicals and the subsequent oxidative stress are considered biotoxic
368 and have the ability to inhibit chondrogenic differentiation (18-21). In the present study,
369 the concentration of ferucarbotran necessary to inhibit the chondrogenic differentiation
370 of MSCs varied across donors, probably due to the variation in the amount of
371 intracellularly incorporated iron among the donors. However, the exposure of
372 magnetically labelled MSCs to the magnetic field (1.5T, 10 minutes) did not affect the
373 chondrogenic differentiation capacity of magnetic MSCs in our previous report (4).

374 To our knowledge, no previous study has investigated the relationship between the iron
375 concentration used for magnetic labeling and MSC reactivity towards magnetic attractive
376 force. In our study, magnetic flux density of 100 mT or more was required for inducing
377 the reactivity of MSCs to the magnetic attractive force. The concentration of
378 ferucarbotran necessary to show the reactivity of MSCs to the magnetic attractive force
379 varied across donors. For donor 1F4287, magnetic labeling at the density of 48.8 μg
380 Fe/mL maintained the chondrogenic differentiation capacity of MSCs as well as the
381 reactivity of MSCs to the magnetic attractive force. On the contrary, magnetic labeling at
382 the density of 97.6 $\mu\text{g Fe/mL}$ maintained the chondrogenic differentiation capacity of
383 MSCs and the reactivity of MSCs to magnetic attractive force in donors 429365 and

384 451491. These were considered appropriate conditions for the magnetic labeling of MSCs
385 for use in cartilage repair. A previous report showed that the labeling of MSCs with iron
386 protamine sulfate is not toxic and does not affect their ability to differentiate (22). Hence,
387 iron protamine sulfate might be helpful for the magnetic delivery system. However,
388 protamine sulphate was not used in the present study because it has not been approved
389 for clinical use of intra-articular administration in Japan.

390 In vivo kinetics of iron particles following the transplantation of magnetically labeled
391 MSCs has been assessed by MRI and Berlin blue staining of tissue sections (23). These
392 iron particles decreased in number at 4 weeks and disappeared at 12 weeks after the
393 transplantation.

394

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400

401 **Conflicts of interest**

402 The authors declare that they have no conflicts of interest.

403

404 **Disclosure Statement**

405 No competing financial interests exist.

406

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493 Address correspondence to:

494 *Naosuke Kamei, MD, PhD*

495 *Department of Orthopaedic Surgery, Division of Medicine, Biomedical Sciences Major,*

496 *Graduate School of Biomedical Sciences, Hiroshima University*

497 *1-2-3 Kasumi, Minami-ku, Hiroshima 734-8551, Japan*

498 *Phone: (+81) 82-257-5233, FAX: (+81) 82-257-5234*

499 *E-mail: nahkamei@hiroshima-u.ac.jp*

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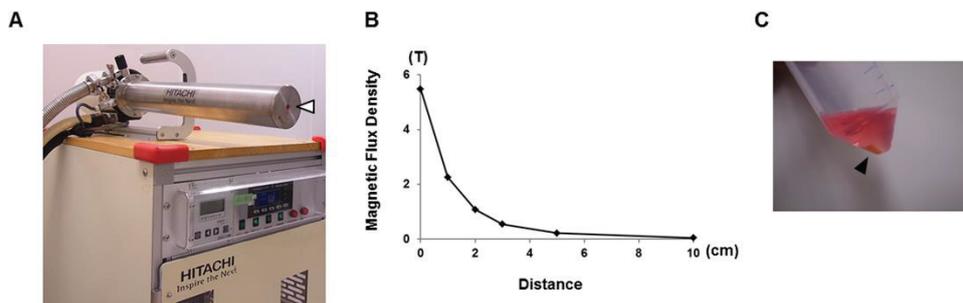
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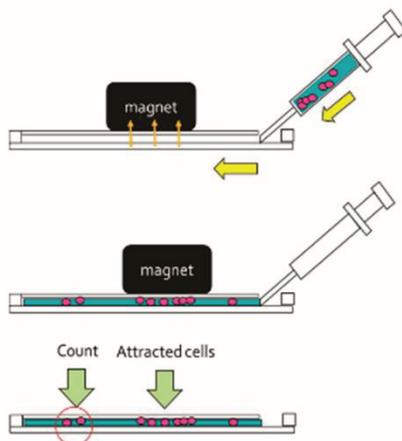
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504 **Figure Legends**

505 **Fig. 1:** (A) The superconducting magnetic device. The white triangle indicates the center
506 of magnet where magnetic flux density is highest. (B) A graph representing the magnetic
507 flux density distribution. (C) The magnetically labeled MSCs were aggregated in a tube
508 after the exposure to magnetic field.

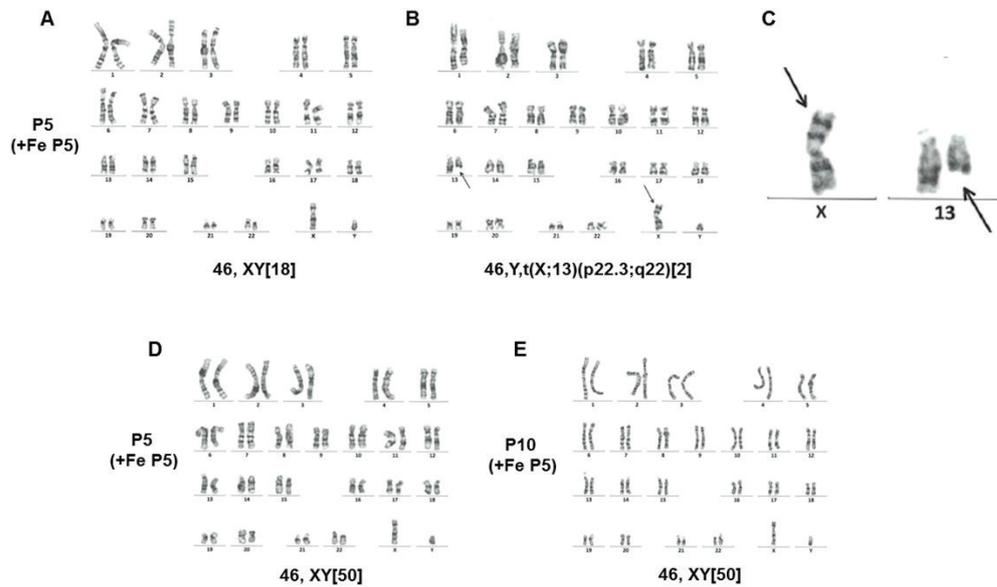


510 **Fig.2** The assessment of reactivity of magnetically labeled MSCs for magnetic attractive
511 force. The eternal magnet is put on the center of the column in the micro fluidics chip.
512 The cell solution is injected into one hole. The MSCs passed under the magnet are counted.

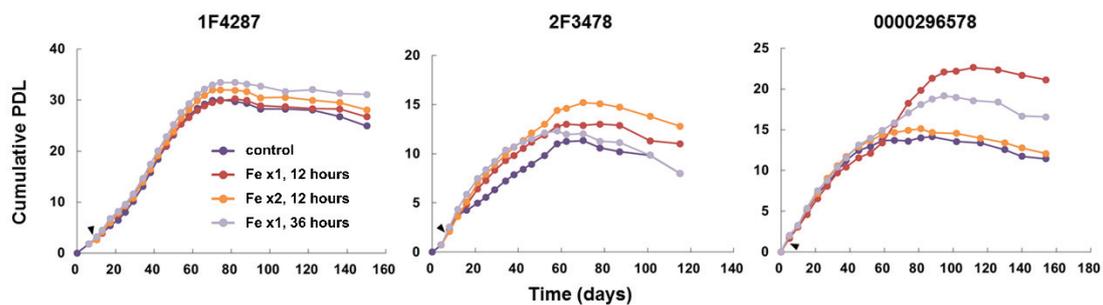


513
514 **Fig.3:** The karyotype analysis in magnetically labeled MSCs from 1F4287. Although 18
515 of 20 P5 MSCs labeled at P5 were normal (A), 2 of 20 P5 MSCs labeled at P5 in
516 1F4287 had an abnormality, balanced reciprocal translocation between chromosome 13

517 and chromosome 10 (B, C). In the re-examination of karyotype in 1F4287 (n = 50), P5
 518 MSCs labeled at P5 (D) and P10 MSCs labeled at P5 (E) were normal.

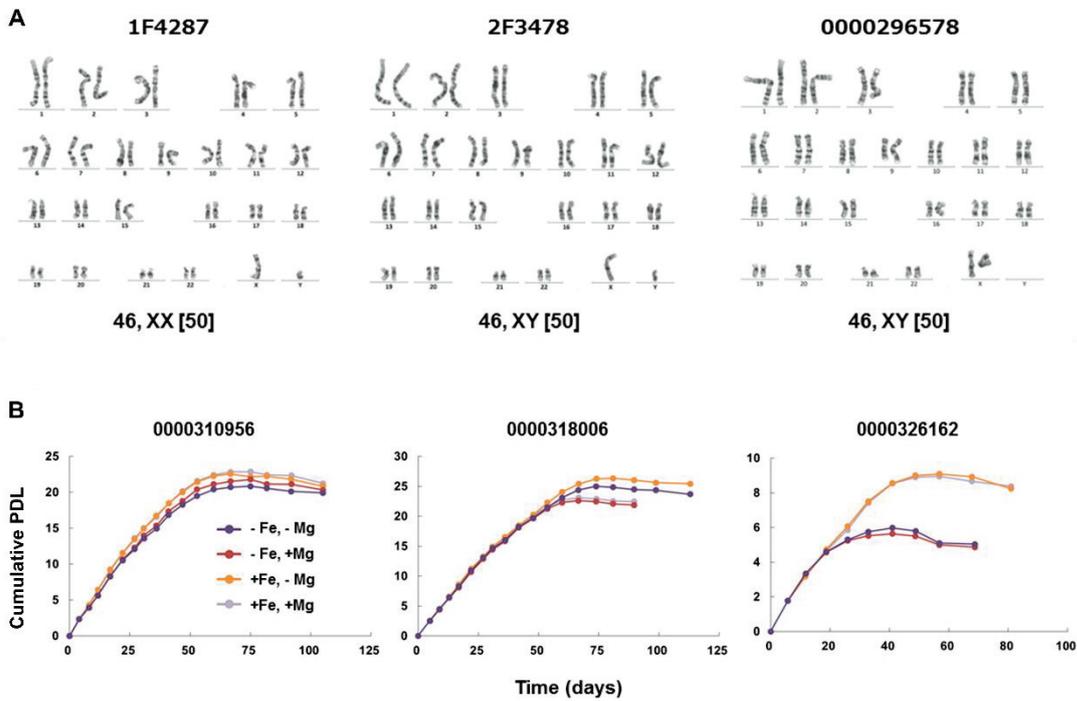


519
 520 **Fig.4:** Plots of cumulative population doublings level (PDL) during long term culture of
 521 labeled MSCs (1F4287, 2F3478, 296578). MSCs were labeled at P3 (arrowhead). “Fe
 522 x1” and “Fe x2” means that cells were labeled by 97.6 µg/mL Fe and 195 µg/mL Fe,
 523 respectively. “12 hours” and “36 hours” means that cells were labeled for 12 hours and
 524 36 hours, respectively. The data represent the average of duplicate values.

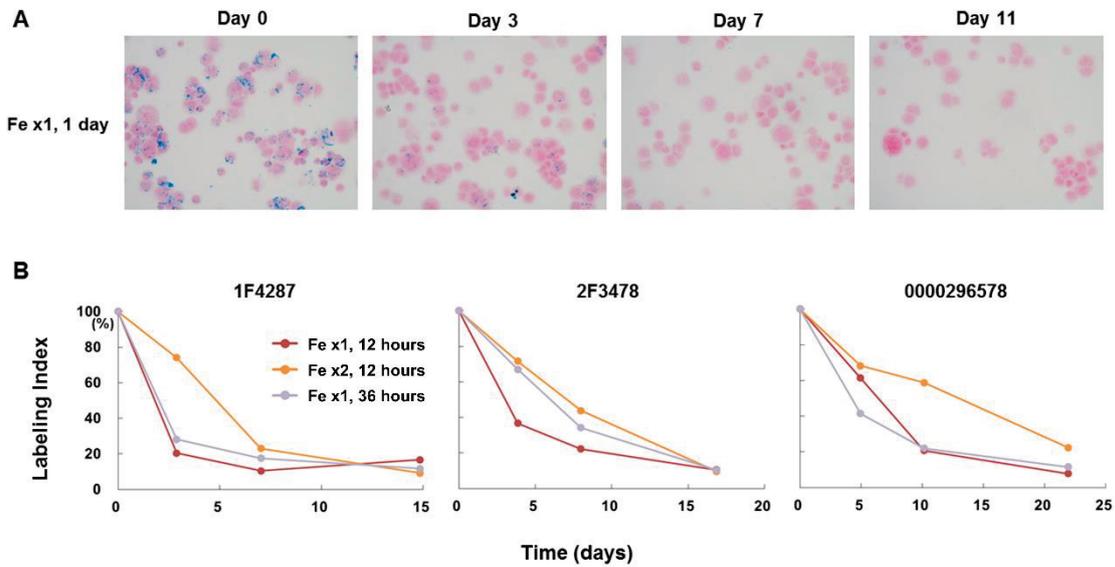


525
 526 **Fig.5:** (A) Karyotype of labeled MSCs exposed to the magnetic field. Abnormality was
 527 never observed in all donors (n = 50; 1F4287, 2F3478, 296578). (B) Plots of cumulative
 528 PDL of labeled MSCs exposed to the magnetic field. “+Fe” and “- Fe” means that the

529 cells were labeled and not, respectively. “+Mg” and “- Mg” means that the cells were
 530 exposed to the magnet field and not, respectively. The data represent the average of
 531 duplicate values.

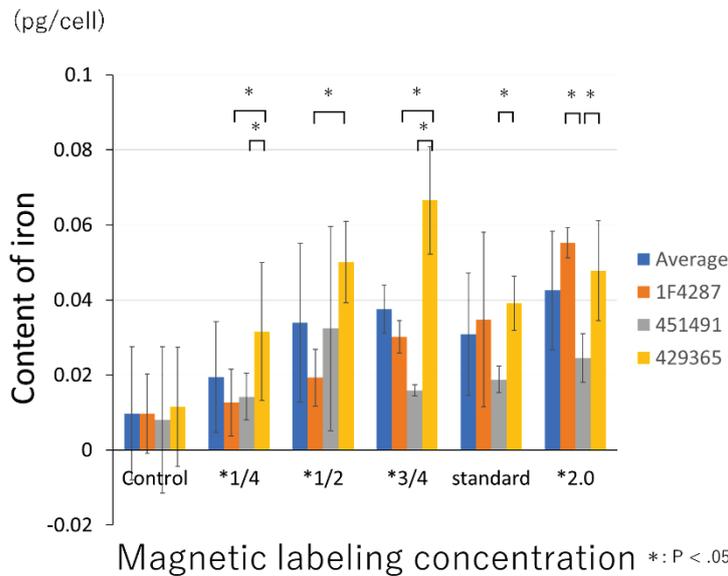


532
 533 **Fig.6:** (A) Berlin blue staining of labeled MSCs (1F4287). Day 0 means just after
 534 magnetic labeling. (B) Quantification of labeling of MSCs. Labeling index is
 535 normalized by the value of day 0 and displayed as relative value. Labeling index
 536 decreased as labeled MSCs were cultured. The data represent the average of duplicate
 537 values.



538

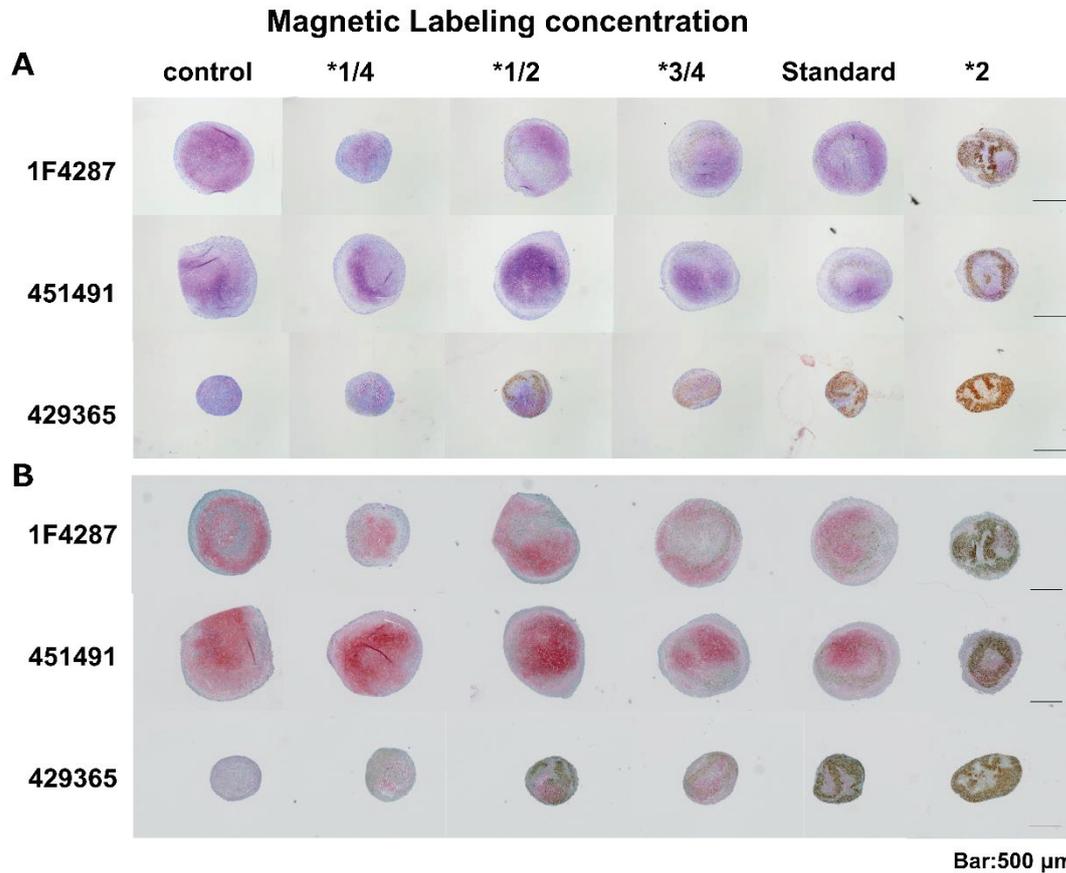
539 **Fig.7:** The content of iron in magnetically labeled MSCs. There were differences of iron
 540 contents in the magnetically labeled MSCs among donors (n = 9). On an average in 3
 541 donors (1F4287, 429365, 451491), the content of iron increased proportionally to the
 542 concentration of ferucarbotran in the medium. The results are represented as mean value
 543 \pm SD.



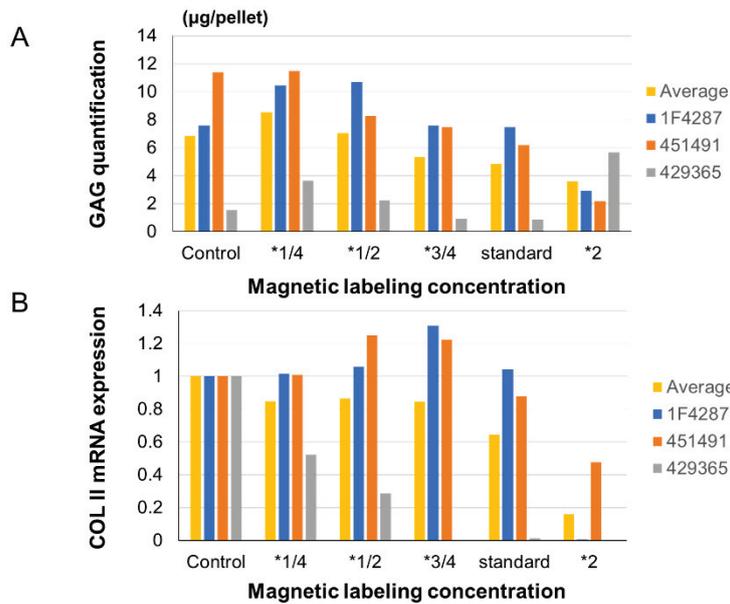
544

545 **Fig.8:** Histological assessments of pellets using the toluidine blue (A) and safranin-O
 546 (B) after chondrocyte differentiation induction of magnetically labeled MSCs (1F4287,

547 429365, 451491). Metachromasia of the pellets from all donors in the twice dose group
 548 are lower than that of the other groups were lower than that of the other groups in the
 549 toluidine blue and safranin-O staining.

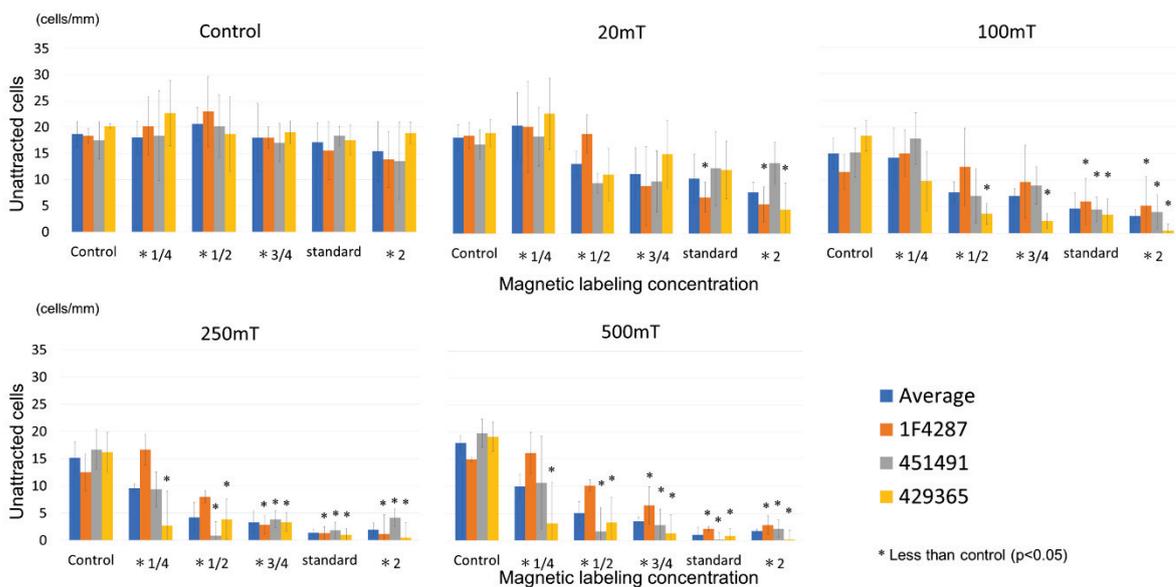


550
 551 **Fig.9:** The quantitative assessments of chondrogenic differentiation of magnetically
 552 labeled MSCs (n = 3, 1F4287, 429365, 451491) using the measurement of
 553 glycosaminoglycan (GAG) (A) and mRNA of collagen type II (COL II) (B). The data
 554 represent the average of duplicate values.



555

556 **Fig.10:** The Reactivity of MSCs labeled in 6 different conditions (0, 24.4, 48.8, 73.2, 97.6,
 557 and 195 $\mu\text{g Fe}/\text{mL}$) for the magnetic field ($n = 6$; 0 mT control, 20 mT, 100 mT, 250 mT,
 558 and 500 mT). A decrease in cell number indicates the attraction of MSCs to the magnet.
 559 The results are represented as mean value \pm SD. Statistical significant differences were
 560 shown only compared with control in the figure.



561