

1       **Device for acoustic measurement of food texture**  
2                               **using a piezoelectric sensor**

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6       **Abstract**

7       We have developed a device that enables direct measurement of food texture. The device  
8       inserts a probe into a food sample and detects the vibration caused by the sample's fracture.  
9       A piezoelectric sensor was used to detect that vibration. The frequency response of the  
10       piezoelectric sensor was measured. Results showed that the sensor covered the full audio  
11       frequency range up to 20 kHz. The device probe was designed so that its resonance was not  
12       in the signal detection band. An octave multi-filter was used to analyze the obtained signals.  
13       Preliminary data were obtained and used to quantify the sample texture. Quantification of  
14       food texture was possible by using the device together with the analytical tool. We also  
15       discuss the application of the device to investigation of physical and structural aspects of  
16       food.

17       *Key words:* acoustic measurement; food texture; piezoelectric sensor

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## 1. Introduction

Food texture, such as crispness, is an important attribute of fresh produce (fruits and vegetables) when consumers assess their quality. However, texture is subjective and depends on the kind of commodity. An effective solution to this problem is to measure quantitative properties of such food texture and provide an objective standard for it. As one step toward the development of a solution, we developed a device that allows us to measure food's textures directly. The device measures the vibration caused by the fracture of the sample when inserting a probe into the sample. Humans are also inferred to sense such vibration and to evaluate the food texture. We used a piezoelectric sensor because piezoelectric sensors have good sensitivity to small signals and excellent responses over a wide frequency range. In addition, we have developed a new probe for the device. The probe is an important component of the device because it directly contacts with a sample to be examined. We carefully designed the probe by giving attention to its resonance frequency because that resonance markedly distorts the signals.

Extensive studies have addressed food texture. A general method of measuring food texture is to study the sounds produced by food mastication. Drake (1963, 1965) was an early researcher to study foods using the method. Then Vickers and Bourne (1976) set a hypothesis that the crispness sensation was produced by sounds. They proposed a model of the cellular structure to explain the generation of crisp sounds. As a crisp cellular material is crushed, a series of sounds is produced. Each sound results from the fracture of a cell or cell wall. However, Christensen and Vickers (1981) proposed that the vibrations produced by fracturing crisp foods might underlie the perception of crispness because a judgment could be made in the absence of auditory cues. Vickers (1981) later concluded that information reaching the brain

1 by either the auditory or the oral route produced very similar crispness judgments.  
2 General discussions of acoustical methods for food texture studies have been re-  
3 viewed by Duizer (2001), and Roudaut, Dacremont, Pamies, Colas and Le Meste  
4 (2002). Most previous studies, including those described above, recorded sounds  
5 produced by food mastication (Edmister & Vickers, 1985; Kapur, 1971; Dacre-  
6 mont, Colas & Sauvageot, 1991; Lee, Deibel, Glembin & Munday, 1988; Seymour  
7 & Hamann, 1988). One inherent problem of this method is that the intrinsic texture  
8 information can be lost because of resonance of the palate or mandible. Further-  
9 more, soft tissues in the mouth absorb or dampen higher frequency sounds (Vick-  
10 ers, 1991). Our device obtained complete signals without such loss because of the  
11 factors stated above. The concept of direct measurement of crispness resembles the  
12 approach by Vincent (1998, 2004), which was to translate “crispness” into a form  
13 that is describable by materials science, and to measure independent parameters at  
14 the material and structural levels.

15 This paper reports the conceptual design of the new device for measuring food tex-  
16 ture and characteristics. We show a tool for analyzing the obtained data with the  
17 device. Preliminary results obtained through the use of this device are included. Fi-  
18 nally, possible improvements to the device and its application to an investigation for  
19 further understanding of food texture were discussed from the aspect of mechanical  
20 fracture.

## 21 **2. The device and system**

22 Human beings mainly use three organs to evaluate food texture: the teeth, the nerves  
23 and the brain. We masticate food using teeth, detect the texture using nerves and  
24 process the signals and perceive the texture of food using the brain. Therefore, a

1 device for measuring food texture should be equipped with these three parts. We  
2 developed a device that satisfies these three aspects (Fig. 1). The device was based  
3 on the experimental setup reported previously by Sakurai, Iwatani, Terasaki and  
4 Yamamoto (2005a, b). In Fig. 1, the probe represents the teeth, the piezoelectric  
5 sensor the nerves, and the computer the brain. The probe was inserted into a food  
6 sample and the sensor detected the vibrations produced by the fracture of the sam-  
7 ple.

8 The probe we used was a stainless steel screw with a conical tip. The probe was  
9 30 mm long, with 5 mm diameter. The probe's tip angle was  $30^\circ$ . The piezoelectric  
10 sensor was a 3-mm-thick discoidal-type unit with 10 mm diameter (Fuji Ceram-  
11 ics Corp., Fuji, Japan). In addition, a 0.4-mm-thick piezoelectric film of 20 mm  
12 diameter was tested. This type is widely used for sounding buzzers. The discoidal  
13 piezoelectric sensor was bonded directly to a 14-mm-diameter aluminum piston  
14 with epoxy adhesive. Figure 1 shows that the piston was housed in a brass cylin-  
15 der. The 80-mm-diameter cylinder was made of brass with 14 mm i.d. A conveying  
16 pump (Hiranuma Sangyo Co. Ltd., Mito, Japan), which contained low-viscosity  
17 silicone oil, drove the probe. The vibration signals obtained with the piezoelectric  
18 sensor were put into a low-noise preamplifier (SR-560, Stanford Research Systems,  
19 Inc., Sunnyvale, CA, USA) and acquired with a computer program developed us-  
20 ing LabVIEW (National Instruments Corp. Ltd., Austin, TX, USA) where the data  
21 sampling rate was 80 kHz. Data were then analyzed in the frequency domain. We  
22 developed an octave multi-filter to perform this analysis using the LabVIEW pro-  
23 gram, as shown in Fig. 2. Frequency bands of the multi-filter were determined using  
24 an octave scale taking into account human auditory sensation. The multi-filter cov-  
25 ered up to 25.6 kHz (full audio frequency range).

26 Using filtered data, we were able to quantify food texture using an algorithm de-

1 veloped previously by Taniwaki, Hanada and Sakurai (2006). The “texture index”  
2 value was determined according to the amplitude density of the obtained signals,  
3 as

$$4 \quad \frac{\sum |V_i|}{T}, \quad (1)$$

5 where  $|V_i|$  is the absolute amplitude of each data point in volts and  $T$  is the data  
6 length in seconds.

### 7 **3. Characterization of the Device and Results**

8 The brass cylinder with low-viscosity silicone oil allowed smooth movement of  
9 the aluminum piston when the probe was driven. This feature minimized the noise  
10 caused by the piston movement. The probe speed was  $22 \text{ mm s}^{-1}$ , which was within  
11 a range of actual mastication speed (Roudaut et al., 2002). The probe was able  
12 to move over a distance of 30 mm, which was sufficiently long to accommodate  
13 insertion of the probe into the food sample.

14 Frequency responses of the piezoelectric sensors were measured as shown in Fig. 3.  
15 Measurement was performed by exciting the piezoelectric sensors with swept sine  
16 signals and by measuring their surface vibration using a laser Doppler vibrometer  
17 (LDV). The LDV measured the surface motion velocity. We converted the velocity  
18 data to displacement data. Figure 3(a) shows the frequency response of the discoidal  
19 3-mm-thick, 10-mm-diameter piezoelectric sensor. We obtained an almost constant  
20 frequency response over the full audio frequency range except for 1 kHz or lower.  
21 However, fluctuations were observed below 1 kHz.

22 Figure 3(b) was taken with the piezoelectric film of 0.4 mm thick and 20 mm in

1 diameter. Using an acrylic holder with a slight gap that allowed the piezoelectric  
2 film to vibrate effectively, the piezoelectric film was sandwiched for testing this  
3 type. Larger displacement was obtained for the same input signals because this type  
4 was much thinner than the discoidal type. An almost constant frequency response  
5 was obtained up to about 6 kHz and in the low-frequency region down to about 20  
6 Hz.

7 Resonances of the probe should be higher than 20 kHz because our frequency of  
8 interest was the full audio frequency range (up to 20 kHz). We designed the probe  
9 so that the lowest resonance frequency was much higher than the observation fre-  
10 quency range, as described in Fig. 4. We estimated the lowest resonance frequency  
11 of the probe of various diameters by assuming, for convenience, that the probe was  
12 cylindrical, but it was actually conical at the tip (Fig. 5). The following standard for-  
13 mula for the lateral mode was used to estimate the lowest resonance of the probes  
14 (Rao, 1990).

$$15 \quad \omega = (\beta l)^2 \sqrt{\frac{EI}{\rho A l^4}} \quad (2)$$

16 In that equation,  $\omega$  represents the angular frequency,  $E$  is the Young's modulus,  $I$   
17 is the area moment of inertia,  $\rho$  is the density,  $A$  is the cross sectional area, and  $l$   
18 is the length. The factor  $\beta l$  was 1.875 for the fixed-free boundary condition (Rao,  
19 1990). We used parameters  $\rho = 7.9 \times 10^3 \text{ kg m}^{-3}$  and  $E = 2.0 \times 10^{11} \text{ Pa}$  for steel.  
20 For the 5-mm-thick and 30-mm-long probe, the estimated resonance was calcu-  
21 lated as 25 kHz. The longitudinal mode frequency was higher than the lateral mode  
22 frequency. Although the actual resonance should be lower than that of the estima-  
23 tion for cylindrical shape, that estimation is useful if it is well above the frequency  
24 range of interest. Furthermore, the brass cylinder was designed to be massive and  
25 sufficiently thick to avoid interfering resonances that would otherwise distort the

1 acquired signals.

2 Figure 6 shows typical signals obtained using the device for an apple sample. Typ-  
3 ical signals can be characterized by near-random variation of the amplitudes in the  
4 time domain. The signals were in a short period of time about 0.6 s when the probe  
5 moved some 10 mm into the sample. Figure 7 (a) shows the calculated texture in-  
6 dices (determined by Eq. 1) for apples, persimmons and pears using filtered texture  
7 signal data. The texture indices were calculated for each frequency band. The re-  
8 sults show that the texture indices for apples were higher than those for persimmons  
9 and pears. It means that the level of sound produced by fluctuation of the samples  
10 was higher over the determined frequency bands for apples than for the others. At  
11 the band of 2240 to 3200 Hz, note that the levels of apples and persimmons were  
12 markedly higher than that of pears. In Fig. 7 (b) the texture indices were normal-  
13 ized by the total amount of indices (total amount = 100) over the frequency bands  
14 to characterize the frequency dependency of the texture indices of the fruit samples.  
15 The normalized indices show significant difference among the fruit samples above  
16 4480 Hz.

#### 17 **4. Discussion**

18 The device developed for measuring food texture mimics the initial bite with the  
19 front teeth. It allows direct measurement of food texture, solving the problem that  
20 some parts of the texture information could be lost in the case of recording the mas-  
21 tication sound as stated in the Introduction. We used a piezoelectric sensor, which  
22 has good sensitivity and a response over a wide frequency range. The dynamic  
23 range of the piezoelectric sensor covered the full audio frequency range (Fig. 3a).  
24 The frequency range of the sound for crisp products was reported to be up to some

1 10-12 kHz (Vickers et al., 1976; Lee et al., 1988; Al Chakra, Allaf & Jemai, 1996).  
2 Therefore, the dynamic range of our piezoelectric sensor should be sufficient for  
3 measuring food crispness. Furthermore, De Belie, De Smedt and De Baerdemaeker  
4 (2000) stated that the higher frequency could be important because a logarithmic  
5 scale can characterize human hearing. In this case, piezoelectric sensors should be  
6 advantageous for their wide frequency response. In addition, we made efforts to  
7 reduce the background noise because the signals produced by the fracture of some  
8 food samples were very small. The silicone oil cylinder connected to the conveying  
9 pump was expected to produce less noise than that driven by an electric motor or  
10 an air-driven pump.

11 Signals obtained with our device contain information related to the food texture.  
12 The signals resembled those of mastication sound data taken by others (Vickers et  
13 al., 1976; Vickers, 1991) using a microphone. However, our data are more informa-  
14 tive because data in some frequency ranges can be lost during recording mastication  
15 sounds. It is important to analyze the obtained signals to extract the information that  
16 represents the food texture. To achieve this, we used the obtained data to quantify  
17 food texture using an algorithm developed by Taniwaki et al. (2006). The normal-  
18 ized texture indices (Fig. 7b) made it possible to compare the texture of different  
19 food samples.

20 Other studies have used the mastication sound amplitude (Drake, 1965), the mean  
21 sound pressure (Seymour et al., 1988), the sound duration (Edmister et al., 1985; Al  
22 Chakra et al., 1996), and the number of sound bursts (Vickers et al., 1976; Edmister  
23 et al., 1985; Vickers, 1987). The sound frequency is also useful for differentiating  
24 between crisp and crunchy products, as stated by Dacremont (1995). The most  
25 widely used frequency analysis method for food texture is the fast Fourier transfor-  
26 mation (FFT) (Lee et al., 1988; Seymour et al., 1988). However, FFT analysis is

1 not appropriate for our data, for example, that shown in Fig. 6. Such signals are in a  
2 very short time period. Therefore, the frequency resolution is limited. Furthermore,  
3 such signal's FFT spectrum characteristics might be unclear because the signals  
4 are non-periodic. We developed the octave multi-filter to overcome such problems  
5 (Fig. 2). This is also an analysis method in the frequency domain.

6 One problem of our device is the piezoelectric sensor's detection range. Figure 3  
7 (a) shows that the discoidal type sensor covers the full audio frequency range in  
8 the high frequency region, but small fluctuations are apparent below 1 kHz. For the  
9 piezoelectric film, the frequency response was better than that of discoidal type  
10 in the low-frequency region (Fig. 3b). However, this type was not good in the  
11 high-frequency region above 6 kHz because of its resonances. Therefore, future  
12 efforts should be made to obtain a good response for the discoidal type sensor in  
13 the low-frequency region. This might be achieved through the use of a multilayered  
14 piezoelectric sensor. We also noticed that the frequency response of the piezoelec-  
15 tric sensor depended strongly on the bonding condition. We used epoxy adhesive  
16 to bond the piezoelectric sensor to the aluminum piston. It was difficult to obtain  
17 exactly the same bonding condition allowing reproduction of the same frequency  
18 response of the piezoelectric sensor. In addition, a different type of probe might be  
19 necessary for different kinds of food samples. For example, a thin knife edge probe  
20 might be preferable for green onions, which are rich in fibrovascular tissues.

21 Our device should be useful for studying food texture. For full understanding of  
22 food texture, Tesch, Normand and Peleg (1996) stated that there must be an under-  
23 standing of how mechanical failure occurs as well as of the resulting sound waves  
24 that occur with this failure. Furthermore, few researchers have studied relationships  
25 between the physical, sensory and structural components of crisp products (Duizer,  
26 2001). Our device should also contribute to solving such problems by investigating

1 physical and the structural components of crisp food. In relation to food structure,  
2 microscopic studies can be performed using our device. Using the probe speed and  
3 the data sampling rate, we can calculate the probe's spatial resolution. That resolu-  
4 tion was calculated as  $0.28 \mu\text{m}$  with a  $22 \text{ mm s}^{-1}$  probe speed and 80 kHz sampling  
5 rate. Typical sizes of a plant cell and a cell wall are respectively about  $100 \mu\text{m}$   
6 and  $1 \mu\text{m}$ . Therefore, it might be possible to detect vibrations or sounds produced  
7 by the fracture of each cell and to measure the cell-wall strength, which should be  
8 responsible for food texture.

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1 **Figure Captions**

2 **Fig. 1.**

3 Device for measuring food texture and the system diagram. Texture signals  
4 were taken by inserting the probe into a sample and by detecting vibrations  
5 caused by the sample fracture. The device has a 3-mm-thick and 10-mm-diameter  
6 piezoelectric sensor. The 30-mm-long, 5-mm-diameter stainless steel probe has  
7 a conical tip.

8  
9 **Fig. 2.**

10 The octave multi-filter developed using the LabVIEW program. Frequency  
11 bands were up to 25.6 kHz, as determined by an octave scale to cover the full  
12 audio frequency range.

13  
14 **Fig. 3.**

15 Frequency responses of the piezoelectric sensors: (a) 3-mm-thick, 10-mm-  
16 diameter discoidal type, and (b) 0.4-mm-thick, 20-mm-diameter thin film type.  
17 Measurements were taken using a laser Doppler vibrometer and converted to dis-  
18 placement data.

19  
20 **Fig. 4.**

21 The probe design concept. The probe resonance should be well above the fre-  
22 quency range of interest because it markedly distorts the signals. In our case, the  
23 frequency range of interest was the full audio frequency range (up to 20 kHz).

24

1 **Fig. 5.**

2 Estimation of the probe resonance for its various diameter and length. The  
3 lowest lateral mode frequency was calculated assuming that the probe was an  
4 aluminum cylinder.

5

6 **Fig. 6.**

7 Typical signals obtained using the device. Signals generally consist of near-  
8 random alternation of amplitude. This example was taken with an apple sample.

9

10 **Fig. 7.**

11 Calculated texture indices for apples, persimmons and pears (a) and the nor-  
12 malized texture indices (b). The texture indices were calculated for each fre-  
13 quency bands using the filtered texture signal data. Vertical bars represent SE  
14 (persimmon,  $n = 21$ ; apple,  $n = 15$ ; pear,  $n = 21$ ).

15

Fig. 1, Taniwaki

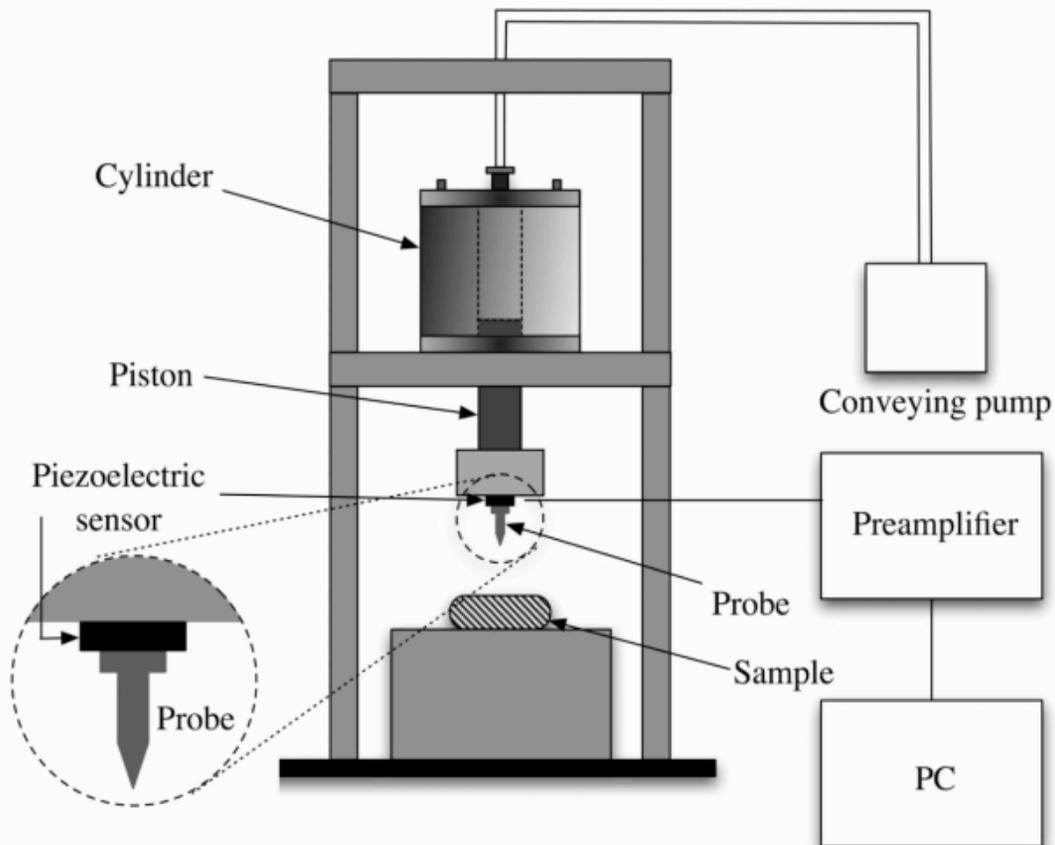


Fig. 2, Taniwaki

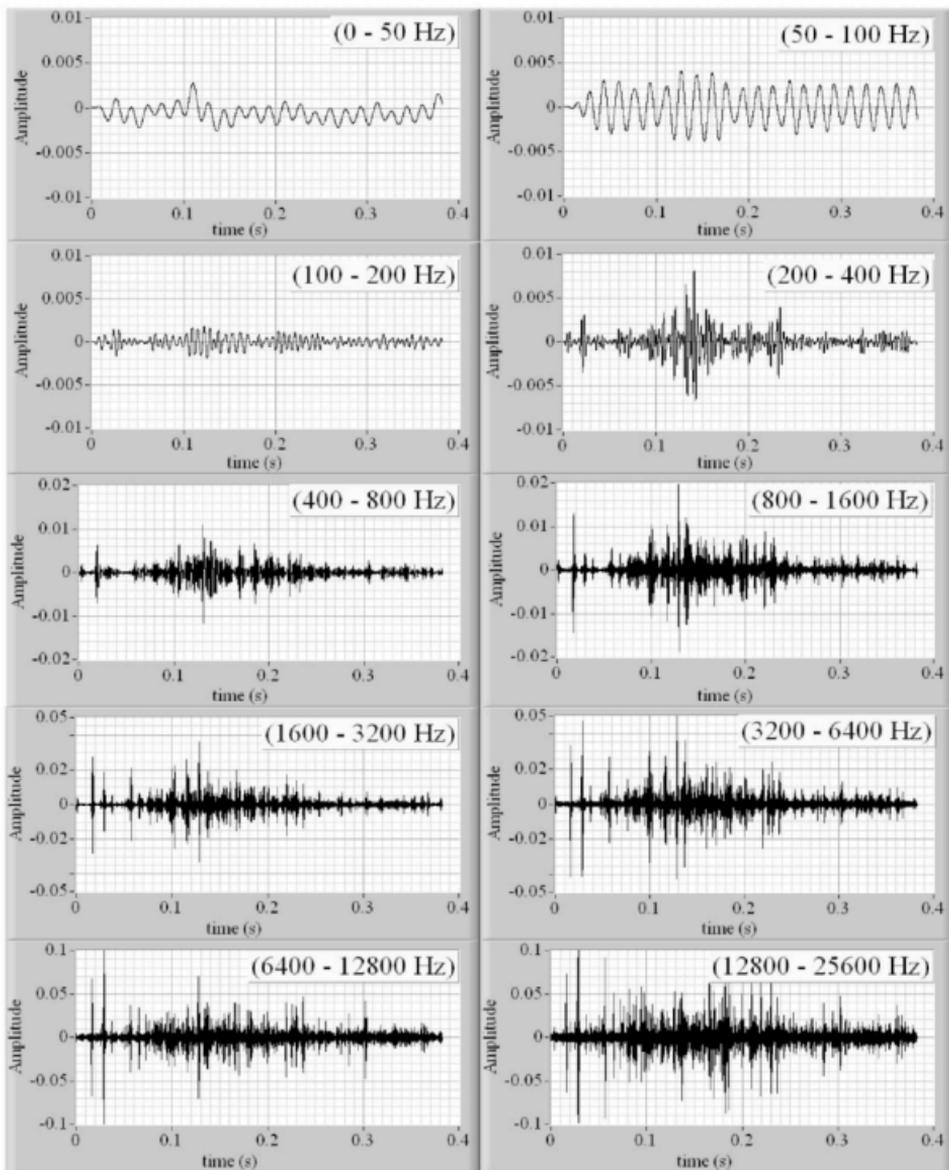


Fig.3, Taniwaki

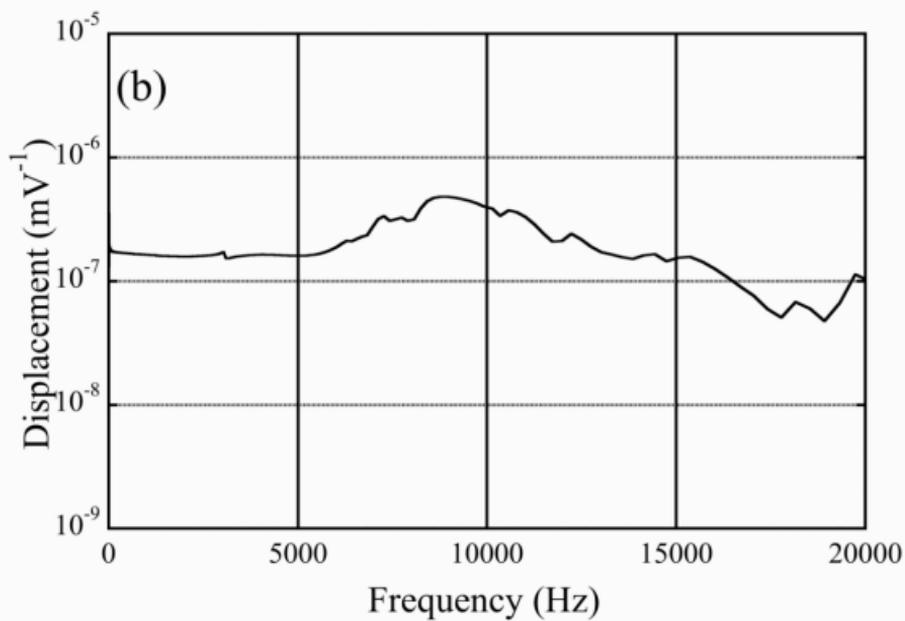
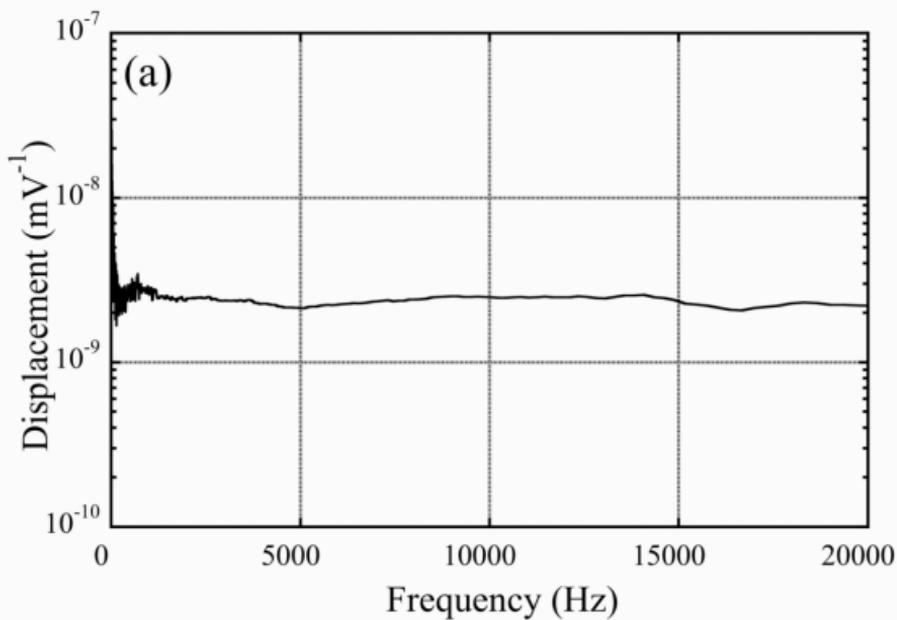


Fig.4, Taniwaki

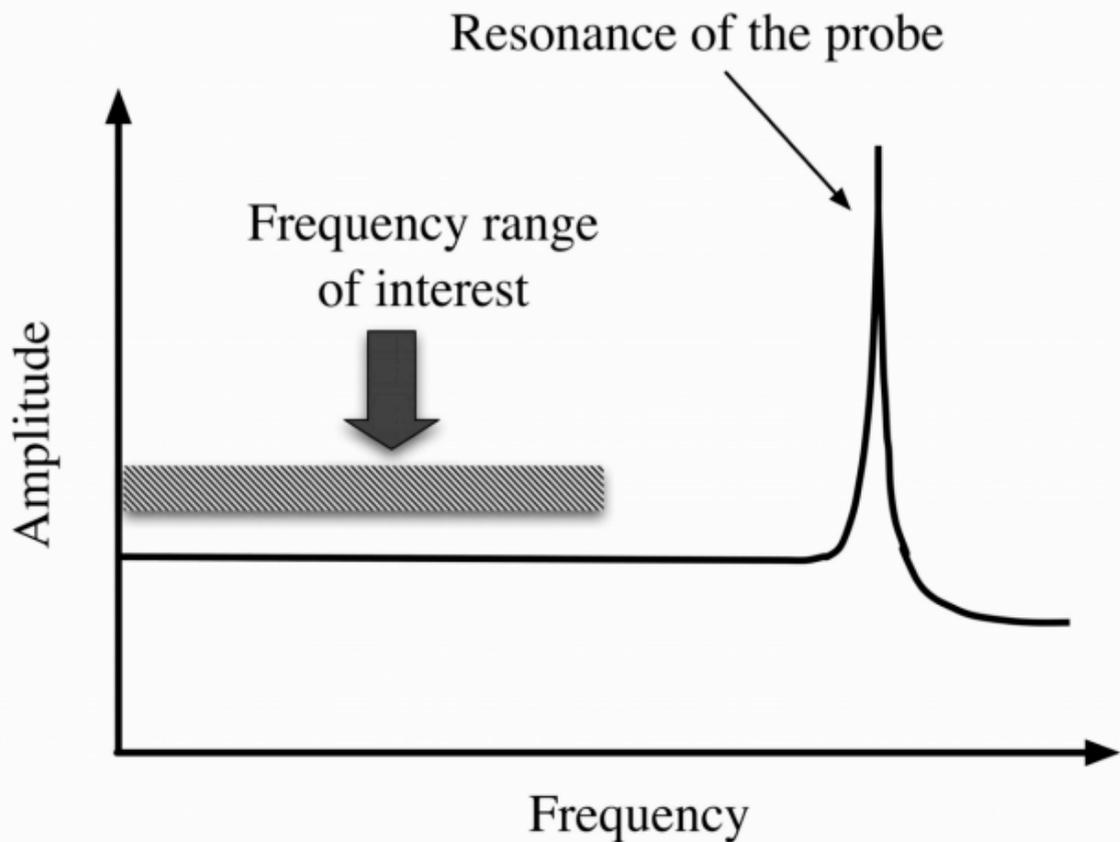


Fig.5, Taniwaki

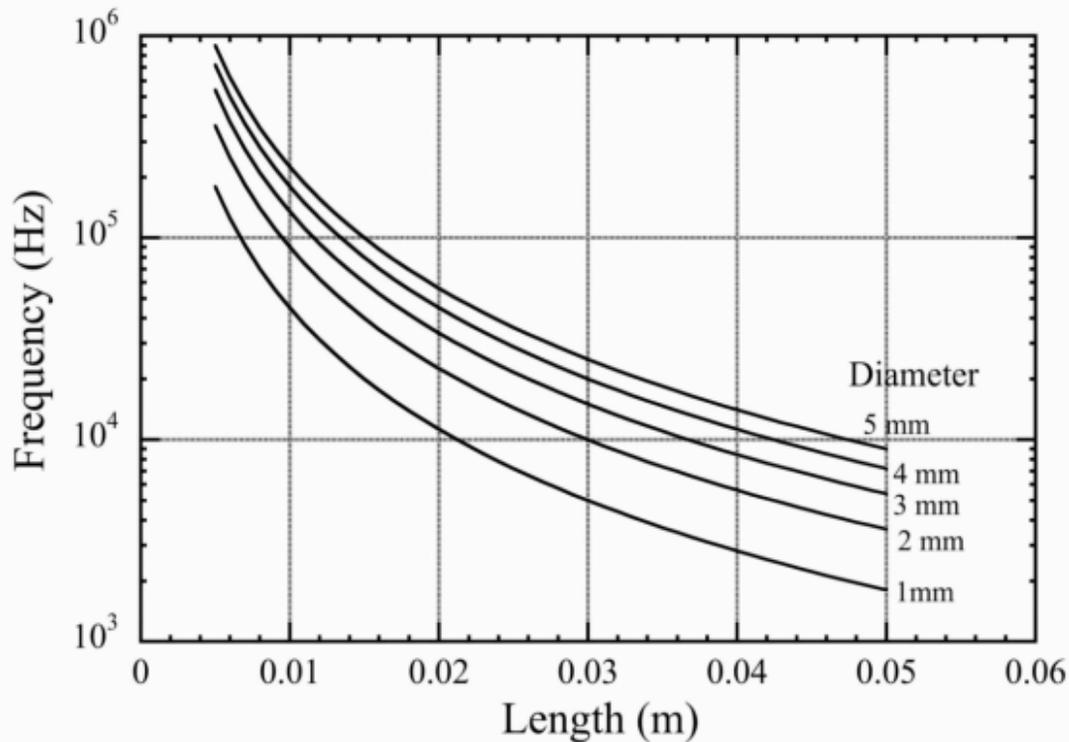


Fig.6, Taniwaki

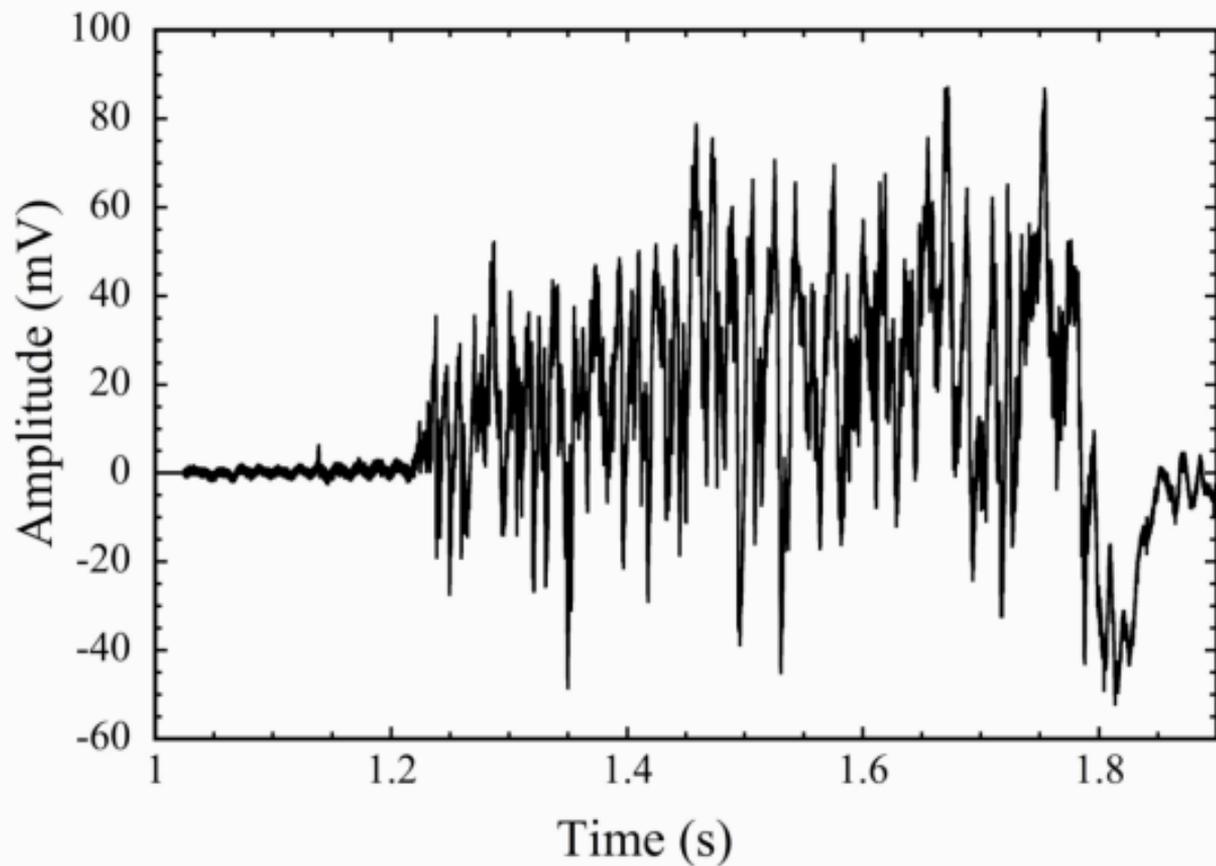


Fig.7, Taniwaki

